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4 Evaluation of Excipients for Enhanced Thermal
5 Stabilization of a Human Type 5 Adenoviral Vector
6 through Spray Drying

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1 **Introduction**

2 Adenovirus-based gene transfer vectors have been increasingly developed as vaccine
3 platforms against both old and newly emerging infections (Lasaro and Ertl, 2009; Majhen et al.,
4 2014; Zhu et al., 2015). However, the real world application of adenoviral vectors, in particular
5 in the developing countries, is limited by their instability when stored or transported at even mild
6 temperatures. Alteration of genetic data within viral genomes for vaccine vector applications
7 results in an increased instability in maintaining infectious function (Amalfitano et al., 1998;
8 Havenga et al., 2006). Storage of these vectors within synthetic vials furthermore accelerates
9 denaturing of proteins and loss of viral infectivity through aggregation. Thus, to maintain
10 function, adenoviral vectors suspended in an aqueous medium require storage at temperatures
11 close to -80°C to maintain 'cold chain' protocols (Nyberg-Hoffman and Aguilar-Cordova, 1999).
12 This condition is critical for inhibiting molecular movements of the stored adenoviruses,
13 hindering their aggregation else resulting in vector inactivation (Kumru et al., 2014; Rexroad et
14 al., 2006, 2003). Immobilization of viral vectors within cold storage conditions are
15 uneconomical, and potentially infeasible in areas around the globe requiring vaccination the
16 most.

17 A major goal for both the World Health Organization and Bill & Melinda Gates
18 Foundation is to alleviate cold chain requirements for vaccine storage and distribution (World
19 Health Organization, 2011). Hence, thermal stability, as used in reference to new classes of
20 vaccines, refers to the ability of a viral vector to be stored at elevated temperatures (above -80°C)
21 for prolonged duration without significant loss of activity. A promising approach capable of
22 increasing thermal stability of labile vectors is through their dispersion within the amorphous
23 phase of a solid matrix, termed as vitrification (Crowe et al., 1997; Rexroad et al., 2003).

1 Vitrification of viral vectors within sugars, polymers, amino acids, surfactants, and other
2 materials has maintained viral activity at storage temperatures above typical cold chain
3 temperatures (Alcock et al., 2010; Amorij et al., 2008; Maa et al., 2004).

4 Previous studies have dictated the importance of matrix physical and chemical properties
5 on thermal stability.(Yu, 2001) The production of a solid matrix is known to greatly hinder the
6 molecular movements of an entrapped adenoviral vector, thus preventing unfolding and
7 aggregation (Ihnat et al., 2005). Selection of a purely amorphous matrix may result in a solid
8 with high moisture sensitivity (Hancock and Zografis, 1993) which will reduce stabilization of
9 any dispersed labile biological materials (Ahlneck and Zografis, 1990). Conversely, crystalline
10 structures are moisture-resistant but not optimal for stabilizing dispersed biological materials due
11 to poor incorporation within the matrix. Binary excipient mixtures are a novel consideration for
12 stabilizing viral vectors since they can be used to balance the physical characteristics of a
13 formulation (Couchman, 1978; Penning and St. John Manley, 1996), though no current examples
14 are systematically evaluated within the literature. The work presented here demonstrates the
15 potential viability for semicrystalline powders as stabilizing matrices. As pharmaceutical
16 excipients require regulatory approval for use, this work highlights that it is not necessary to be
17 even more restrictive in excipient selection by not considering crystalline and semicrystalline
18 materials. Furthermore, crystallinity may offer material advantages, as previous publications
19 have demonstrated that crystalline regions can act as physical barriers for molecular movements
20 and water sorption (Bronlund and Paterson, 2004; Mihranyan et al., 2004; Mizuno et al., 1998).
21 The present work evaluates two binary sugars and one amino acid formulation to observe the
22 effects of crystallinity and excipient glass transition temperature (T_g) on adenovirus stabilization.

1 Several drying processes such as spray drying, freeze drying and foam drying have been
2 employed in recent years for producing dry powder forms of solid viral vector dispersions (Jin et
3 al., 2010; Ohtake et al., 2010; Wong et al., 2007). Spray drying is increasingly preferred since its
4 simple requirements facilitate product scalability (Ré, 1998) and favorable economics. During
5 spray drying, a pressurized gas is used to disperse a liquid feed into small droplets within a
6 drying chamber. Evaporation of heated aqueous droplets results in precipitation of the dissolved
7 solutes and suspended materials. Current research aimed at improving thermal stability for labile
8 biological materials has shown great success with spray drying vaccines ranging from attenuated
9 pathogens to antigen-based formulations (Garmise et al., 2007; Jin et al., 2010; Ohtake et al.,
10 2010; Saluja et al., 2010; Wong et al., 2007). The degree of thermal stabilization varies
11 significantly depending on the dispersed biological material. For example, a spray dried bacillus
12 Calmette-Guérin vaccine formulation with L-leucine demonstrated a minimal activity loss of
13 approximately 2.0 log after 120 days at 25°C under high moisture protection (Wong et al., 2007).
14 Alternatively, an antigen-based influenza subunit vaccine stabilized in inulin retained
15 considerable immunogenicity for up to three years of storage at 20°C (Saluja et al., 2010). The
16 variance in stability among spray dried biological materials emphasizes the need for specific
17 evaluation of each vaccine backbone and excipient combination.

18 Human adenovirus type 5 (AdHu5) has been shown to be an effective vaccine vector for
19 prevention of infectious diseases and has been developed in both liquid buffer and lyophilized
20 forms (Frahm et al., 2012; Smaill et al., 2013). Current limitations to AdHu5 use stem from pre-
21 existing AdHu5 immunity and the lack of a thermally stabilized form. It is estimated that 30 -
22 100% of the population, depending on geographical location, have been exposed to AdHu5 and
23 therefore elicit an AdHu5-specific response upon infection (Appaiahgari and Vrati, 2014). The

1 anti-AdHu5 immunity pre-existing in most of the human population poses a potential limitation
2 to the application of AdHu5-vectored vaccines. However, the results from our recent clinical
3 vaccine trial suggest that the potency of AdHu5 vector system is able to diminish the negative
4 effect of a pre-existing immunity (Smaill et al., 2013). Furthermore, AdHu5 vector is particularly
5 amenable to vaccination via the respiratory mucosal route against lung infectious diseases and
6 the human respiratory tract has been found to have minimal pre-existing anti-AdHu5 immunity
7 (Richardson et al., 2011). Thus, it is expected for AdHu5-based vaccine to be even more
8 effective when given via the respiratory mucosal route versus a parenteral route. In terms of
9 thermal stability, AdHu5 has yet to be developed into a well-stabilized spray dried form. This
10 work extends the possible applications of AdHu5 as a vaccine by producing a more thermally
11 stable vector through spray drying with well-accepted excipients. More specifically, we have
12 evaluated binary sugar and amino acid formulations consisting of semicrystalline and entirely
13 crystalline excipient matrices to observe the effects of crystallinity and T_g on AdHu5 stability.
14 The effects of storage time, temperature and humidity were systematically examined on spray
15 dried vector infectivity for AdHu5, which to the best of our knowledge, has not been reported
16 previously. The purpose of this work is to demonstrate a thermally stable spray dried AdHu5
17 vector and highlight the physical properties necessary for the best stabilization, which can be
18 used to further the field of dry powder vector development. Future developments with these
19 spray dried powders will focus on their use for inhalation and optimizing excipient ratios for
20 better thermal stability of the labile material. The future use of these spray dried powders in
21 inhalable applications is dependent on a suitable safety assessment, as the effects of
22 administration of the studied excipients within this work to the lungs has not been fully
23 established.

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Materials and Methods

Chemicals and Adenoviral Vectors

Anhydrous lactose, D-(+)-trehalose dihydrate, D-mannitol, dextran (M_w 40000 kDa) and L-leucine were all purchased as USP grades from Sigma-Aldrich (Ontario, Canada). Culture media was produced from α -minimum essential medium (prepared in the lab according to protocol by Life Technologies (Ontario, Canada)) with 10% fetal bovine serum and 1% streptomycin/penicillin (Invitrogen; Ontario, Canada). X-Gal stock solution was purchased from EMD Millipore (Ontario, Canada). A recombinant replication-defective human type 5 adenovirus expressing *Escherichia coli* β -galactosidase (AdHu5LacZ) was produced in the vector facility of McMaster Immunology Research Centre as described previously (Xing et al., 1996).

Spray Drying

Spray dried powders were produced using a Büchi Mini Spray Dryer B-290 (Büchi; Switzerland) with 0.7 mm spray nozzle and high performance cyclone. The setup is shown schematically in Figure 1, consisting of 1) the spray drying nozzle, 2) the drying chamber, 3) the separating cyclone and 4) the collection chamber. The atomizing air was dried using an in-line silica gel desiccant air dryer (McMaster-Carr; Elmhurst, IL) and cleaned using an Aervent® 0.2 μ m filter (EMD Millipore; Billerica, MA). Three excipient formulations were produced: (1) L-leucine, (2) 90% lactose and 10% trehalose and (3) 67% mannitol and 33% dextran (all compositions are quoted based on percent by weight). Excipient formulations were dissolved in Milli-Q® water. The AdHu5 vector was stored in a PBS buffer; however, its addition to the

1 excipient solution was negligible, being less than 1/10000th of the spray dried volume. The input
 2 concentration of viral vector for each formulation was 7.56 x 10⁶ TCID₅₀/mg. The pH of the
 3 solution was 6.5. The formulations used within this work were selected from a number of
 4 excipients that have been employed within the pharmaceutical and spray drying industry (Amorij
 5 et al., 2008; Ohtake et al., 2010; Vehring, 2008; Wu et al., 2014; Yu, 2001) and can be found in
 6 the Inactive Ingredient Database for Approved Drug Products (FDA). The reported formulations
 7 (Table 1, in terms of excipients used and excipient ratio) were derived from preliminary spray
 8 drying experiments (results not included) that looked to achieve a high yield of non-
 9 agglomerating particles with matrices of significant amorphous content and high glass transition
 10 temperatures. The specific spray dryer conditions used for each formulation were based on those
 11 preliminary experiments attempting to minimize the adenoviral vector activity loss through
 12 processing. Recovery was calculated as a percentage of the mass of powder in the collection
 13 vessel compared to the input amount. All spray drying processes and powder collection were
 14 performed in a custom biosafety cabinet (Design Filtration; Ontario, Canada).

15 **Table 1.** Spray drying process parameters and powder recovery for each formulation.

Parameter	L-leucine	90% Lactose/10% Trehalose	67% Mannitol/33% Dextran
Solid Concentration (mg/mL)	3 ^a	10	10
Spray Gas Flow (L/h)	439.11	666.93 ^b	439.11
Inlet Temperature (°C)	90	90	120 ^c
Outlet Temperature (°C)	54	48	65
Feed Flow Rate (mL/h)	145.0	145.0	217.5 ^d
Recovery (%)	81.4	83.1	84.5

16 *a: Formation of crumpled L-leucine particles after spray drying prevented concentrations of 10 mg/mL.*

17 *b: Increased spray gas flow for lactose/trehalose formulation increased powder production without any observed decrease in*
 18 *viral titre post-spray drying.*

19 *c,d: Greater inlet temperature and feed flow rate increased post-spray drying viral titre.*

20

21 **Sample Storage**

22 Powder samples were stored for different durations at relative humidities (RH) of <10%,

23 45% and >90%. Storage humidity was produced with gel desiccants and saturated salt solutions

1 (potassium carbonate, 45% RH; potassium nitrate, >90% RH) within desiccators. The relative
 2 humidity within each compartment was confirmed before sample observation through direct
 3 measurement with a Fisher Scientific™ Traceable™ Jumbo Thermo-Humidity Meter (Fisher
 4 Scientific; Ontario, Canada), and found to vary $\pm 3\%$. The liquid control containing only buffer
 5 and AdHu5LacZ was stored in a tightly sealed vial under ambient conditions due to the
 6 dehydrating effects of desiccants and saturated salts, though it is assumed that humidity would
 7 have no effect on the liquid sample. All aging trials examining the influence of humidity were
 8 performed at 20°C. Samples and storage conditions are listed in Table 2. Sealed samples were
 9 stored in closed 2 mL Nalgene General Long-Term Storage Cryogenic Tubes (Nalgene; Ontario,
 10 Canada).

11

12 **Table 2.** Storage conditions and corresponding sample formulations.

Storage Condition			Samples Stored
Temperature	Relative Humidity	Storage Time	
20°C	<10% RH	Up to 90 days (evaluated at 0, 1, 10, 45 and 90 days)	L-leucine Lactose/Trehalose Mannitol/Dextran
20°C	45% RH	Up to 90 days	L-leucine Lactose/Trehalose Mannitol/Dextran
20°C	>90% RH	15 days	L-leucine Lactose/Trehalose Mannitol/Dextran
20°C	Sealed, ambient humidity	Up to 90 days	Liquid Control
37°C	Sealed, ambient humidity	Up to 72 hours	Liquid Control Mannitol/Dextran
45°C	Sealed, ambient humidity	Up to 72 hours	Liquid Control Mannitol/Dextran
55°C	Sealed, ambient humidity	Up to 72 hours	Liquid Control Mannitol/Dextran

13

14 **Particle Size and Morphology**

15 Spray dried particle size and morphology was examined using a JEOL JSM-7000F
 16 scanning electron microscope (SEM) (JEOL Ltd.; Japan). Samples containing adenovirus vector

1 were inactivated through exposure to UV light for 30 minutes prior to imaging. All samples were
2 applied to double-sided tape and coated with a 5.0 nm layer of platinum. Micrograph images
3 were collected at several magnifications at a working distance ranging from 10.0-10.3 mm and
4 an electron accelerating voltage ranging from 3.0-5.0 kV. All electron microscopy was
5 conducted at pressures less than 5.0×10^{-4} Pa. SEM images were analyzed using ImageJ
6 (Abràmoff et al., 2004) to measure the dimensions of nodular masses found on particle surfaces.

7 A Malvern Mastersizer 2000G (Malvern Instruments; United Kingdom) equipped with a
8 He-Ne laser was used to measure particle size and size distribution. Powder formulations were
9 dispersed in anhydrous ethanol at concentrations of 0.3 mg/mL, 1.0 mg/mL and 1.0 mg/mL for
10 L-leucine, lactose/trehalose and mannitol/dextran formulations, respectively. Mean powder
11 particle size was determined as the average diameter (n=3), and represented as Feret diameters as
12 powders are not entirely spherical. Powder size span was calculated using Equation 1, where
13 D(0.9) represents the diameter greater than 90% of measured particles, D(0.1) represents the
14 diameter greater than 10% of measured particles and D(0.5) represents the median diameter.

$$Span = \frac{[D(0.9) - D(0.1)]}{D(0.5)} \quad (1)$$

15

16 **X-ray Photoelectron Spectroscopy**

17 Surface elemental analysis was performed using a Physical Electronics (PHI) Quantera II
18 X-ray photo electron spectrometer (Physical Electronics; Chanhassen, MI). Samples containing
19 adenoviral vectors were inactivated through exposure to UV light for 30 minutes. X-rays were
20 generated using an Al source and focused with a quartz crystal monochromator. A
21 monochromatic Al K- α X-ray (1486.7 eV) source was operated at 50W 15kV with a spot size of
22 $200 \mu\text{m}$ and at pressures less than 2.67×10^{-6} Pa. Each recorded measurement was a survey

1 spectra average of five sample scans. Data manipulation and analysis was performed using PHI
2 MultiPak software (Physical Electronics; Chanhassen, MI).

3 Argon etching was accomplished using a 500V beam of Ar to bombard the surface of
4 each specimen. Approximately 100 nm was removed from each sample using etch rates based
5 off of computer simulated Monte Carlo calculations (Williams et al., 2003).

6

7 **Moisture Uptake of Spray Dried Particles**

8 For analysis of moisture content, aged spray dried powders without the adenoviral vector
9 were dissolved in formamide and injected into a Mettler Toledo DL39 Coulometric Karl Fischer
10 Titrator (Mettler Toledo; Columbus, OH). The corresponding water content was determined
11 using Equation 2:

$$\text{Water content [ppm]} = x \cdot \frac{f2 + f3}{f3} - \frac{f1 \cdot f2}{f3} \quad (2)$$

12 where x was the measured water content of the sample after Karl Fischer titration (ppm), and $f1$
13 was the water content of the solvent used (ppm). Water content of the formamide solvent was
14 measured by adding formamide without dissolved solids to the Karl Fischer titrator. $f2$ was the
15 measured mass of solvent (g) and $f3$ represents the mass of dissolved sample (g).

16

17 **Thermal Properties of the Spray Dried Particles**

18 Thermograms for the three excipient formulations (without adenoviral vector) were
19 measured using a differential scanning calorimeter (DSC). Samples of 3-10 mg were weighed
20 into hermetically sealed aluminum pans for analysis in a Q200 Differential Scanning Calorimeter
21 (TA Instruments; New Castle, DE). The procedure for measurement involved first equilibrating
22 the sample at 4°C. Sample was heated to 300°C at a ramp rate of 10°C/min under a nitrogen

1 purge gas flowing at 50 mL/min. The heating rate was established from a previous study
2 characterizing lactose and trehalose samples (Mazzobre et al., 2001). Thermal events were
3 recorded from a single heating ramp to avoid dehydration of the sample.

4

5 **Crystallinity of Spray Dried Particles**

6 The excipient formulations (without adenoviral vector) were characterized by powder X-
7 ray diffraction (XRD) on a Bruker D8 Discover with DAVINCI.DESIGN diffractometer (Bruker;
8 Billerica, MA) using a Cobalt Sealed Tube Source ($\lambda_{\text{avg}} = 1.79026 \text{ \AA}$, $2\Theta = 5-70^\circ$). Small sample
9 quantities were mounted on a silica base for examination. A blank silica sample signal was
10 subtracted from each measured data set using GADDS software (Bruker; Billerica, MA), and the
11 resulting signal intensity was integrated into a crystallographic figure through the use of
12 DIFFRAC.EVA software (Bruker; Billerica, MA). Crystalline content was determined using
13 TOPAS software (Bruker; Billerica, MA).

14

15 ***In Vitro* Testing of Spray Dried Particles**

16 **Culturing of A549 Cells**

17 A549 lung epithelial cells were thawed from liquid nitrogen and cultured in T150 culture
18 flasks using Alpha Minimum Essential Medium Eagle (α -MEM). All cell culturing was
19 completed in a humidified Forma Series II Water Jacketed CO₂ Incubator (Thermo Scientific
20 Corporation; Waltham, MA) at 37.0°C and 5.0% CO₂. When cells were 80-90% confluent, they
21 were split to a new T150 flask and/or plated in a 96-well plate for *in vitro* testing.

22

23

1 **Effect of Excipient Formulations on *In Vitro* Experiments**

2 Approximately 10 mg of each spray dried formulation (without adenoviral vector) was
3 dissolved within 100 μ L of culture media and added to A549 epithelial cells plated within a 96-
4 well plate through the use of a Gilson micropipette (Gilson; Middleton, WI). The concentration
5 of 10 mg/100 μ L was chosen because it is three times more than the concentration used for *in*
6 *vitro* infection (3 mg/100 μ L). Control samples contained only 100 μ L of culture media. Cells
7 were left to incubate for 24 hours. After incubation, A549 cells were trypsinized and tested for
8 viability through use of a trypan blue solution (Life Technologies; Ontario, Canada). Cell
9 suspensions were mounted on a Bright-Line™ hemacytometer (Reichert; Buffalo, NY) and the
10 number of viable and nonviable cells were counted. Results are reported as percentage of viable
11 cells measured and error bars represent the standard deviation (n=3).

12

13 **Spray Dried Formulation Viral Infectivity**

14 The retained viral activity or infectivity of AdHu5LacZ vector after spray drying and
15 storage was determined by infecting plated A549 cells with approximately 3 mg of spray dried
16 powder (input concentration of 7.56×10^6 TCID₅₀/mg) reconstituted in culture media right before
17 testing. Eight-fold serial volume dilutions were created from each reconstituted sample, ranging
18 from a dilution of 10^{-1} to a dilution of 10^{-8} or ranging from a dilution of 10^0 to a dilution of 10^{-7} .
19 Cells were incubated with AdHu5LacZ for 24 hour, and then fixed using a 0.2% glutaraldehyde
20 (Sigma Aldrich; Ontario, Canada)/0.8% formaldehyde (Sigma Aldrich; Ontario, Canada)
21 solution in phosphate buffered saline (%v/v) for less than five minutes. After removal of fixative,
22 viral infection was detected as X-gal color reaction indicative of the cells transduced by
23 infectious AdHu5LacZ viral particles present in the dried powder using the substrate 5-bromo-4-

1 chloro-3-indoyl β -(D)-galactoside (X-gal). The number of cells positive for color reaction was
2 determined using an Axiovert 25 inverted light microscope (Zeiss; Germany). Median tissue
3 culture infectious dose (TCID₅₀) was then calculated using the Reed-Muench method as detailed
4 within the literature (Reed and Muench, 1938). Results are reported as loss of viral activity (log
5 TCID₅₀/mg) and error bars are calculated as the standard deviation (n=3).

6

7 **Data Analysis**

8 Where applicable, results were statistically analyzed using the statistical package R (R
9 Foundation for Statistical Computing; Austria). Results were considered statistically significant
10 for $p \leq 0.05$.

11

12 **Results and Discussion**

13 **Characterization of Spray Dried Powders without Adenoviral Vector**

14 **Size and Morphology**

15 The spray dried powder formulations were imaged by SEM at varying magnifications to
16 evaluate size and morphology, as shown in Figure 2. L-leucine particles were generally less than
17 10 μm in diameter (Figures 2a and 2b), with an average of 8.80 μm (Table 3). The size
18 distribution was broadest for L-leucine compared to the other formulations and had a noted
19 skewness in the Mastersizer favoring smaller particles. These particles had a "collapsed sphere"
20 morphology as a result of the hydrophobic isobutyl side chain on L-leucine which enhanced its
21 surface activity (Gliński et al., 2000), causing reduced diffusion within the drying droplet. This
22 results in an early onset of particle precipitation and the formation of hollow spheres that are
23 prone to collapse, as seen with the L-leucine formulation. Both lactose/trehalose (Figures 2c and
24 2d) and mannitol/dextran (Figures 2e and 2f) formulations showed spherical morphologies when

1 spray dried. These latter cases are indicative of systems with a lower Peclet number due to their
 2 enhanced solubility and reduced surface activity (Elversson and Millqvist-Fureby, 2005).
 3 Average particle diameter for the lactose/trehalose and mannitol/dextran powders were 32.2 μm
 4 and 7.92 μm , respectively (Table 3). The larger average particle size for the lactose/trehalose
 5 formulation can be attributed to a greater amount of agglomeration between developed particles
 6 (notable by the bridging outlined in Figures 2c and 2d). The span in the size distribution for these
 7 two formulations were smaller, as indicated in Table 3, compared to L-leucine and both showed
 8 a more normal distribution of sizes according to the Mastersizer around their means.

9 **Table 3.** Average spray dried particle size and span (calculated by equation 1), measured by
 10 Mastersizer, for the three formulations tested.

Formulation	$D_{50} (\mu\text{m})$	Span
L-leucine	8.80	2.05
Lactose/Trehalose	32.2	1.73
Mannitol/Dextran	7.92	1.61

11

12 **Moisture Uptake**

13 The measured water content after storage under different humidity conditions is plotted in
 14 Figure 3 for the three spray dried formulations. For the 15 day evaluation, the least hygroscopic
 15 spray dried powder was produced with the L-leucine formulation. Total moisture content for L-
 16 leucine (measured as percent weight of the total) was 0.98%, 1.98% and 6.76% under controlled
 17 relative humidity conditions of <10, 45 and >90% RH, respectively. In comparison, the
 18 lactose/trehalose formulation absorbed significant amounts of water, measured as 2.54%, 4.21%
 19 and 17.08% for <10, 45, and >90% RH, respectively. A similar amount of moisture uptake was
 20 determined for the mannitol/dextran formulation; at <10, 45, and >90% RH, the respective 15
 21 day measurements were 1.72%, 5.89% and 15.05%.

1 Many pharmaceutically relevant excipients have hydrogen bonding potential, allowing
2 for the binding of water from their surrounding environment (Newman et al., 2008). The
3 absorption of water within solid dispersions is generally deleterious, destabilizing their physical
4 structure by depressing the T_g and inducing changes within the crystalline structure. As a result,
5 minimal moisture uptake is optimal for the dispersed active ingredient to remain immobilized for
6 as long as possible (Ahlneck and Zografis, 1990; Hancock and Zografis, 1994). The low water
7 sorption capacity of L-leucine particles is due to the high crystalline content Both lactose and
8 trehalose are considered to be highly hygroscopic materials and hence, it was not unexpected that
9 the spray dried particles from these ingredients similarly showed high moisture uptake in the
10 experiments. Mannitol is typically crystalline and non-hygroscopic (Naini et al., 1998), yet the
11 inclusion of dextran produced spray dried particles with high moisture sensitivity.

12 All spray dried powders showed no significant change in moisture content after day 1
13 when stored at 45% RH or less. In comparison, when stored at >90% RH the powders continued
14 to uptake water and showed no evidence of approaching an equilibrium condition within the
15 tested 15 day period. The spray dried powders stored at >90% RH proved too difficult to
16 preserve in their current state for the detailed characterizations that follow that they will not be
17 reported on further. These powders agglomerated into large masses and were very sticky,
18 proving to be difficult to work with and unsuitable for AdHu5 stabilization.

19

20 **Crystallinity**

21 The three spray dried powders were analyzed by X-ray diffraction as shown in Figure 4.
22 The crystal structure differences were attributed to the different chemical composition of each
23 formulation. Measured crystalline content is shown in Table 4 for each formulation immediately

1 after spray drying. The crystallinity for L-leucine was very high, as the particle was mostly
2 crystallized. Both lactose/trehalose and mannitol/dextran formulations were measured to be
3 semicrystalline.

4 **Table 4.** Measured crystallinity for all formulations immediately after spray drying.

Formulation	Measured Crystallinity (%)
L-leucine	>97%
Lactose/Trehalose	56%
Mannitol/Dextran	44%

5
6 Figure 4a displays diffraction patterns for the crystalline structure of spray dried L-
7 leucine. L-leucine has a propensity to crystallize (Banno et al., 2004), and the sharp peaks in the
8 diffractogram indicate a highly regular crystalline structure was immediately present after spray
9 drying as well as after two weeks of storage at 20°C and <10% RH. Under conditions of 20°C
10 and 45% RH, a small amount of peak broadening was observed for L-leucine. This broadening
11 corresponds with a marginal increase in water content at these conditions, suggesting absorbed
12 water may have partially dissolved and/or disrupted the L-leucine crystal structure.

13 The diffraction patterns in Figure 4b for the lactose/trehalose formulation displayed
14 crystalline α -lactose monohydrate peaks as well as a large amorphous band, when powders were
15 tested immediately after spray drying. The absence of diffraction peaks for α,α -trehalose
16 dehydrate was unexpected due to its high crystallizing nature and from the fact that its crystalline
17 form has been reported after freeze drying (Sundaramurthi and Suryanarayanan, 2010) but in this
18 case its low concentration likely prevented detection by XRD. The significant amorphous
19 content shown was expected having been previously reported for spray dried lactose (Lerk,
20 1993) and furthermore, blends of lactose and trehalose are known to inhibit crystallization in the
21 complementary component (Miao and Roos, 2005). It has been previously reported that the
22 presence of trehalose in a lactose system delayed and prevented lactose crystallization through

1 interference of growth of the crystal lattice (Mazzobre et al., 2001). After storage at 20°C for two
2 weeks, the crystalline regions were less apparent by XRD, even at low humidity. The work of
3 other authors has demonstrated that the onset of crystallization for lactose and trehalose blends
4 occur at 65.6% RH (Miao and Roos, 2005), thus storage of these powders at 45% RH and <10%
5 RH does not allow sufficient moisture for a thermodynamically equilibrated crystal structure to
6 emerge. The broadening of diffraction peaks at these conditions coincided with a decrease in
7 crystallinity similar to what happens when water is lost from a crystalline trehalose structure,
8 resulting in a mostly amorphous material (Ding et al., 1996). This effect of dehydration on
9 crystal structures has been previously reported under mild conditions for both raffinose- and
10 trehalose-based systems (Saleki-Gerhardt et al., 1995; Willart et al., 2002). This process should
11 be anticipated more so in spray dried systems, where the particle is trapped in an unfavourable
12 state as a result of fast drying (Vehring et al., 2007). The broad peaks in Figure 4b (ii, iii) were
13 attributed to the small-sized crystal domains detected by DSC (Rani et al., 2006; Willart et al.,
14 2002).

15 Figure 4c shows the diffraction patterns for the mannitol/dextran formulation. As
16 expected based on other studies (Taylor et al., 1959), dextran exhibited no crystalline peaks in
17 XRD. The crystalline peaks of mannitol were shifted in the presence of dextran, though most
18 closely resembled the α -polymorphic form (Hulse et al., 2009). After two week storage at 20°C
19 and <10% RH, no change in crystallinity was observed. When stored at 20°C and 45% RH, a
20 single broad mixed-mode peak was found as a result of the significant water uptake shown in
21 Figure 3. Both α - and β -polymorphic forms of pure mannitol are reportedly structurally stable in
22 the presence of high RH for several weeks, though under those condition, crystallinity is
23 gradually decreased (Hulse et al., 2009). The relatively hygroscopic nature of dextran leading to

1 greater water uptake, and the previous reports of mannitol crystal disruption from cosolutes such
2 as dextran may have caused this (Kim et al., 1998).

3 Overall, the presence of moisture is detrimental to the structural stability of the matrix as
4 seen by changes in crystal structure for all three excipient formulations. These changes in crystal
5 structure are indicative of movements on the molecular scale, which correspond to activity loss
6 in spray dried particles containing adenoviral vectors, as discussed further below.

7 8 **Thermal Properties**

9 The thermal transitions of spray dried particles from each of the three formulations were
10 analyzed by DSC. The glass transition temperature and peak fusion/sublimation temperature (T_m)
11 are given in Table 5. Spray dried L-leucine particles had sufficiently high crystallinity that the
12 glass transition temperature could not be detected. An endothermic peak at 247°C corresponded
13 to the sublimation of L-leucine (Martins et al., 2006). Both lactose/trehalose and
14 mannitol/dextran formulations exhibited relatively high T_g values immediately after spray
15 drying, measured at 115°C and 130°C, respectively. The T_m of 214°C for lactose/trehalose
16 indicated a depressed melting point that was 8°C below the α -form of crystalline lactose
17 (Listiohadi et al., 2009). The T_m of mannitol/dextran was 162°C, lower than the 170°C reported
18 for pure mannitol (Hulse et al., 2009).

19 After storage for two weeks at 20°C and under dry conditions (<10% RH), the
20 lactose/trehalose and mannitol/dextran powder T_g did not change noticeably, as shown in Table
21 4. However, after storage for two weeks at 20°C and intermediate humidity conditions (45%
22 RH), the T_g for lactose/trehalose and mannitol/dextran decreased significantly to 15°C and 45°C

1 respectively. The decrease in measured T_g is caused by the plasticizing effect of absorbed water
 2 (Hancock and Zografi, 1994).

3 The T_m and especially T_g were key parameters in determining matrix stability in terms of
 4 immobility. Simply stated, higher T_g and T_m were preferred due to the higher ambient
 5 temperatures necessary to induce destabilizing molecular movement

6 **Table 5.** Measured glass transition temperature (T_g) and fusion/sublimation temperature (T_m) for
 7 three formulations.

Formulation	Day 0		Day 15: 20°C/0% RH		Day 15: 20°C/45% RH	
	T_g	T_m	T_g	T_m	T_g	T_m
L-leucine	- ^a	246.8°C	- ^a	252.5°C	- ^a	247.0°C
Lactose/Trehalose	114.8°C	213.8°C	113.8°C	213.7°C	17.6°C	208.1°C
Mannitol/Dextran	127.3°C	162.4°C	127.3°C	162.8°C	45.9°C	153.5°C

8 ^a: L-leucine particles exhibited no detectable T_g .
 9

10 **Effect of Excipient Formulations on *In Vitro* Experiments**

11 To ensure accurate viral infection measurements, the base spray dried formulations
 12 without adenoviral vector were tested for their relative toxicity to the plated A549 cells. The
 13 powders were tested at a concentration level that was three times higher than that for later *in*
 14 *vitro* testing. Cell viability corresponding to each formulation is shown in Table 6. No
 15 cytotoxicity was observed for the three formulations based on the absence of any significant
 16 differences in cell viability between the formulations and the control (α -MEM).

17
 18 **Table 6.** Measured A549 cell viability (%) after 24 hour incubation with each formulation (mean
 19 \pm SD, n=3).

Formulation	Measured Viable Cells (%)
L-leucine	98 \pm 3
Lactose/Trehalose	97 \pm 1
Mannitol/Dextran	98 \pm 2
Control	96 \pm 2

20

21 **Evaluation of Spray Dried Particles Containing Adenoviral Vector**

1 **Retained Viral Activity After Spray Drying**

2 Spray dried powders containing human type 5 adenoviral vector expressing *Escherichia*
3 *coli* β -galactosidase (AdHu5LacZ) were prepared and were indistinguishable in initial
4 appearance from the powders without the viral vector. The high temperatures and shear rates
5 experienced during the spray drying process could presumably lead to some loss in viral
6 infectivity and as such, the vector activity for each formulation was tested immediately after
7 spray drying. As shown in Figure 5, while the L-leucine formulation resulted in a relatively large
8 loss in activity (2.6 ± 0.5 log), the lactose/trehalose and mannitol/dextran formulations exhibited
9 excellent retention of adenoviral vector infectivity with less than 1.0 log loss. The activity loss
10 for spray dried mannitol/dextran with AdHu5 particles was the smallest within this report, being
11 only 0.3 ± 0.1 log. For all three formulations, the collected powder recovery after spray drying
12 was greater than 80% (Table 1) which was important because it implied an efficient processing
13 method where there was no significant loss of valuable biological material, such as the
14 AdHu5LacZ vector tested here.

15 SEM micrographs of spray dried particles containing the adenoviral vector are shown in
16 Figure 6, demonstrating differences in the extent to which the virus was incorporated within each
17 matrix. The large AdHu5 activity loss observed for L-leucine particles may be due to phase
18 separation of the excipient and the adenoviral vector. Nodules were observed at the powder
19 surface (highlighted by black arrows in Figure 6a) which may imply that some AdHu5 is not
20 fully encapsulated. This is in contrast to the L-leucine particles spray dried without AdHu5
21 shown in Figure 2a and 2b. These nodules were measured to be 99 ± 8 nm in diameter which is
22 similar to the reported AdHu5 vector diameter of 70-100 nm (Kennedy and Parks, 2009).
23 Separation could occur due to the high Peclet conditions of L-leucine during spray drying and

1 the “expelling” nature of forming crystals. Due to the low solubility of L-leucine molecules,
2 supersaturation at the droplet surface is thought to occur early in the drying process (Vehring et
3 al., 2007). Furthermore, a crystalline material is unlikely to form stabilizing bonds with any other
4 material, as it is instead more favourable to continue the crystal structure without faults (Jackson,
5 1984). The coupling of high Peclet conditions and poor labile material stabilization in a
6 crystalline product explains the greater loss of AdHu5 activity after spray drying with L-leucine.
7 In Figure 6b, the addition of the adenoviral vector to the spray dried lactose/trehalose
8 formulation also resulted in nodules on the particle surface, although these nodules were $330 \pm$
9 90 nm in diameter, much larger than the AdHu5 vector. These nodules, which were not seen in
10 Figure 2 for particles without AdHu5LacZ, could indicate surface localization of the adenoviral
11 vector, now better encapsulated within a layer of excipient than found with L-leucine. This
12 interpretation of the morphology appears consistent with the infectivity data since the viral
13 vector would have been better isolated from the environment than within L-leucine particles yet
14 not quite so well shielded as in mannitol/dextran. No nodules were visible on the
15 mannitol/dextran particles containing AdHu5 (Figure 6c) indicating complete incorporation.

16 To improve confidence as to the source of the nodule morphology, the surface
17 characterization technique XPS was used to detect nitrogen as a marker for AdHu5LacZ because
18 this element is not present in lactose, trehalose, mannitol or dextran. Testing by this technique
19 was not done with L-leucine since no element could be identified as a unique marker in this case.
20 The adenoviral vector was unlikely to be solely localized in the nodules but the presence of the
21 nodules suggested closer proximity to the particle surface if they did in fact contain AdHu5LacZ.
22 Nitrogen was detected once out of three tests at the surface of the lactose/trehalose particles and
23 once again out of five tests after argon etching away a surface layer of 100 nm in thickness. The

1 same number of tests were conducted with mannitol/dextran particles, with nitrogen never being
 2 detected. The surface elemental composition for a selected test of the AdHu5LacZ control and
 3 both lactose/trehalose and mannitol/dextran powders is shown in Table 7. Due to the detection
 4 threshold of the XPS instrument, a concentration of the AdHu5 vector along the tested surface is
 5 necessary for nitrogen to be shown in the result. As this is not always the case, it is at times not
 6 possible to detect nitrogen. We propose that this method of surface detection for AdHu5 is not
 7 entirely concrete, however it offers a valuable insight into potentially observing viral vector
 8 locations on formed particles. More confident results with higher resolution could be attained
 9 through more rigorous testing, but this would require significant time and resources and is
 10 outside the scope of this project. However, the description of the nodules as containing
 11 AdHu5LacZ seems compelling based on these SEM and XPS results, and provides a reasonable
 12 explanation, in part, for the differences in thermal stability noted between these three excipient
 13 formulations.

14

15 **Table 7.** Elemental composition by XPS for lactose/trehalose and mannitol/dextran samples
 16 (n=8) before and after argon etching 100 nm into the sample.

Formulation	% Composition Pre-etch			% Composition Post-etch		
	C	O	N	C	O	N
AdHu5LacZ Control ^a	46.4	32.3	9.8	-	-	-
Lactose/Trehalose	51.8	48.2	0.0	52.0	47.8	0.7 ^b
Mannitol/Dextran	57.6	42.4	0.0	58.9	41.1	0.0

17 ^aOnly relevant elements are listed for AdHu5LacZ Control. Salt ions from PBS are not listed.

18 ^bNitrogen content was present in two lactose/trehalose samples of eight.

19

20 To highlight the fact that the presence of nodules indicating poorly incorporated AdHu5
 21 can only be part of the explanation for the differences in thermal stability seen in the tests, the
 22 measured viral infectivity loss of only 0.7 ± 0.1 log for the lactose/trehalose formulation needed
 23 to be reiterated. The greater activity retained with this formulation compared to L-leucine is

1 attributed to the exceptional stabilizing profile of trehalose with other bioactive compounds
2 (Mazzobre et al., 1997). The total encapsulation of AdHu5LacZ in mannitol/dextran powders is
3 correlated to the low activity loss after spray drying. As described previously, particle formation
4 is affected by diffusion of the excipient components in aqueous solution during spray drying.
5 Dextran diffusion is heavily restricted compared to lactose and trehalose, which are much
6 smaller sugars (Uedaira and Uedaira, 1985). Thus precipitation at the droplet surface likely
7 begins with dextran, providing less opportunity for adenovirus segregation to the outer particle
8 surface. These results highlight that the chemical nature of the excipients plays a role in their
9 ability to trap and stabilize AdHu5 vector and that morphological inspection of spray dried
10 particles offers further insight into the ability of some formulations to maintain viral infectivity
11 better than others.

12

13 **Viral Infectivity after Storage at 20°C and Differing Humidity**

14 Figure 7 shows the resulting adenoviral vector titre loss through storage at 20°C at <10%
15 RH for each spray dried formulation up to 90 days. For the liquid control (AdHu5LacZ in
16 buffer), significant AdHu5 vector infectivity was lost after 42 days at 20°C and there was no
17 measurable activity after 90 days. This relatively rapid loss of adenoviral vector activity
18 corresponds to previously reported data (Alcock et al., 2010) and further highlights the need for
19 vector stabilization at temperatures above the normal cold chain storage conditions of -80°C. All
20 excipient formulations outperformed the liquid control. However, the mannitol/dextran
21 formulation was able to retain higher viral activity than the other formulations at day 90 for the
22 low humidity condition ($p < 0.01$). The measured AdHu5 titre loss at day 90 was 0.7 ± 0.3 log
23 with mannitol/dextran-formulated vector, only slightly higher than the 0.3 ± 0.1 log measured

1 directly after spray drying. Adenoviral vectors stabilized within lactose/trehalose did not
2 maintain the same degree of function as those stabilized within mannitol/dextran. After 90 days,
3 the measured loss of infectivity for these samples was measured at 3.1 ± 0.3 log. Similarly, L-
4 leucine exhibited poor excipient stability as the measured activity loss on day 90 was 4.0 ± 0.2
5 log. For all formulations, the vector activity loss was greatest within the first two weeks. This
6 was likely due to the greater amount of molecular movements within the particle as it
7 transitioned to an equilibrated state post-spray drying.

8 Figure 8 shows the loss of AdHu5LacZ infectivity for each spray dried formulation
9 during storage for up to 90 days at 20°C under moderate moisture conditions (45% RH). By day
10 90, all formulations were considered to be inactive. This represents a significantly greater viral
11 activity loss at 45% RH compared to <10% RH (noted above) which is attributed to the uptake of
12 water by the spray dried powders within the enclosed storage system. Hygroscopic sugars, and
13 even non-hygroscopic L-leucine particles, will take up detectable quantities of water from the
14 humid air (as demonstrated in Figure 3). As measured by XRD, the crystallographic profiles for
15 both lactose/trehalose and mannitol/dextran powders showed increasing disorder with water
16 uptake over time. XRD peaks from L-leucine particles exhibited only slight broadening
17 indicating disruption of the initially crystalline spray dried structure. Matrix destabilization was
18 further emphasized by the decrease in T_g observed for lactose/trehalose and mannitol/dextran
19 samples (Table 5). This significant decrease in T_g indicated a greater molecular mobility within
20 the stored samples. Overall, the increase in moisture resulted in an accelerated rate of viral titre
21 loss. Whereas in drier conditions the rate of titre loss leveled off after approximately ten days
22 (referring to Figure 7), the same is not observed at 45% RH. This emphasizes the need to store
23 potential AdHu5 vaccines in low humidity environments, however this is more easily maintained

1 than -80°C temperatures and can be done, for example, using blister packs which are common
2 practice in the pharmaceutical industry.

3 Overall, the best-performing powder throughout the storage tests was mannitol/dextran
4 which also encapsulated the adenoviral vector without producing nodules after spray drying (as
5 measured by SEM and XPS). The high T_g for lactose/trehalose particles implied a great thermal
6 stability should have been expected but this was not observed. This could best be explained
7 through the excipient matrix instability as observed through XRD (Figure 4b). The glass-like
8 state is known to be thermodynamically unfavourable as the polymer glass is being held with a
9 higher volume and entropy than its equilibrium state (Farhoodi et al., 2012; Struik, 1977).
10 Physical aging of amorphous and semicrystalline materials can potentially cause a slow
11 relaxation to a more thermodynamically favourable state, even at temperatures below the glass
12 transition (Struik, 1977). This change occurs more significantly in lactose/trehalose particles than
13 mannitol/dextran particles. These molecular movements result in a greater loss of adenoviral
14 vector function throughout storage. Although similar instability is not observed for L-leucine
15 through XRD, a failure to properly incorporate the AdHu5LacZ vector within the matrix renders
16 it a poor excipient formulation for long term storage.

17

18 **Viral Infectivity at Elevated Temperatures**

19 Generally, the mannitol/dextran formulation outperformed the other excipients in its
20 ability to retain adenoviral vector activity under mild storage conditions. This formulation was
21 thus subsequently used to test the thermal stability of AdHu5LacZ at more extreme temperatures
22 of 37°C, 45°C and 55°C. As shown in Figure 9, spray drying adenoviral vector with the
23 mannitol/dextran formulation was found to thermally stabilize the virus significantly more than

1 the liquid control after 72 hours of storage at increased temperatures ($p < 0.05$). For the liquid
2 control, there was no measurable AdHu5LacZ activity after 30 minutes at 45°C, or for any
3 harsher storage conditions. In contrast, the mannitol/dextran formulation exhibited good activity
4 after 72 hours at both 37°C and 45°C. Only at a storage temperature of 55°C was there a
5 significant loss of viral infectivity after 72 hours for the mannitol/dextran particles. This was due
6 to the increase in energy within the system, which promotes viral protein unfolding (Pace and
7 Hermans, 1975; Pace and Vanderburg, 1979). This effect is more pronounced in liquid control
8 samples because there is more molecular movement possible. It is presumed from these results
9 that the mannitol/dextran matrix sufficiently restricts the molecular-scale movements of
10 AdHu5LacZ through immobilization within the vitrified particle, as seen previously for dried
11 influenza viral vaccines (Amorij et al., 2008).

12

13 **Conclusions**

14 In conclusion, this work has demonstrated that spray drying is able to produce a high
15 yield of powders capable of incorporating AdHu5 vectors in amino acid or sugar matrices. These
16 matrices allow for an increase in viral vector infectivity, compared to the liquid control, even
17 when the powders are stored at high temperatures. Thermal stability is influenced by particle
18 morphology; amorphous structures can form secondary bonds with the viral vector leading to
19 immobilization which prevents protein unfolding and aggregation. While some degree of matrix
20 crystallinity can aid in avoiding moisture uptake, which in turn restricts both molecular
21 rearrangements and decreasing T_g , highly crystalline excipients exhibited viral nodules on the
22 spray dried particle surface and a subsequent decrease in viral activity. The significant loss of

1 viral vector activity in highly crystalline matrices can be avoided through incorporation of a
2 semicrystalline structure, where amorphous content is able to stabilize the AdHu5 vector.

3 Improved thermal stability is most pronounced with mannitol/dextran formulations,
4 where the viral vector was fully encapsulated by the matrix and the semicrystalline morphology
5 remained relatively constant over mild storage conditions. More specifically, particles containing
6 AdHu5 and mannitol/dextran are considered almost fully active after storage for 90 days at 20°C
7 with less than 10% RH, as well as after short term storage at extreme temperatures (stable for 72
8 hours at 45°C and 24 hours at 55°C). This represents a substantial improvement in thermal
9 stability compared to AdHu5 stored in a liquid buffer matrix.

10 AdHu5-based vectors have been exploited to develop novel vaccines for a number of
11 important infectious diseases (Lasaro and Ertl, 2009; Majhen et al., 2014; Zhu et al., 2015). For
12 instance, we have found a intramuscular dose of 10^8 pfu AdHu5-based TB vaccine to be safe and
13 effective in a phase 1 clinical trial (Smaill et al., 2013). The effective dose of future inhalational
14 applications in humans is expected to be even smaller than the intramuscular dose. Such doses
15 are within the range of production capacity by using our best currently developed spray drying
16 technology. Furthermore, an increased initial concentration of AdHu5 in each formulation can be
17 explored through future studies. Overall a processing method and matrix formulation were
18 developed to allow AdHu5-based vaccines to be stored above typical cold chain temperatures,
19 making their deployment more straightforward and at a fraction of the cost compared to current
20 viral storage methods. However, relative humidities above 45% were detrimental to maintaining
21 viral activity due to moisture uptake and increased mobility of the matrix. As a result, spray dried
22 particles with adenoviral vectors should be stored in low humidity conditions using dry
23 packaging examples already existent in the industry (Rubio et al., 2008, 2006). Although a

1 semicrystalline matrix was not able to perform exceptionally well at elevated relative humidities,
2 the potential for a semicrystalline stabilizing matrix is apparent at low relative humidities.
3 Extending on this, it may be beneficial to further examine binary mixtures in the future for
4 AdHu5 thermal stability. This is a significant step towards long term storage of AdHu5 vectors
5 with increased thermal stability.

6

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14

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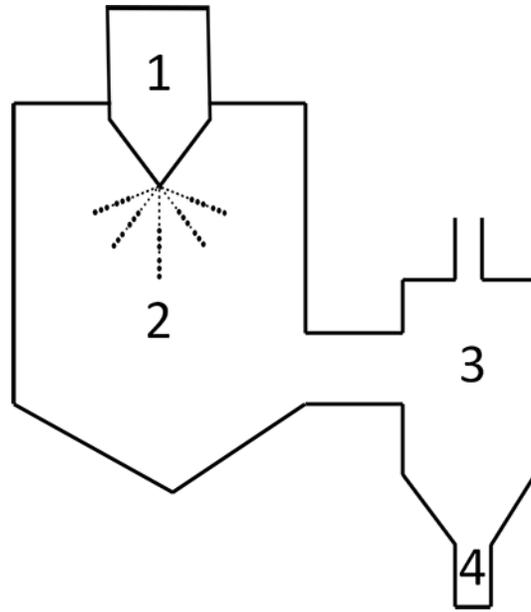
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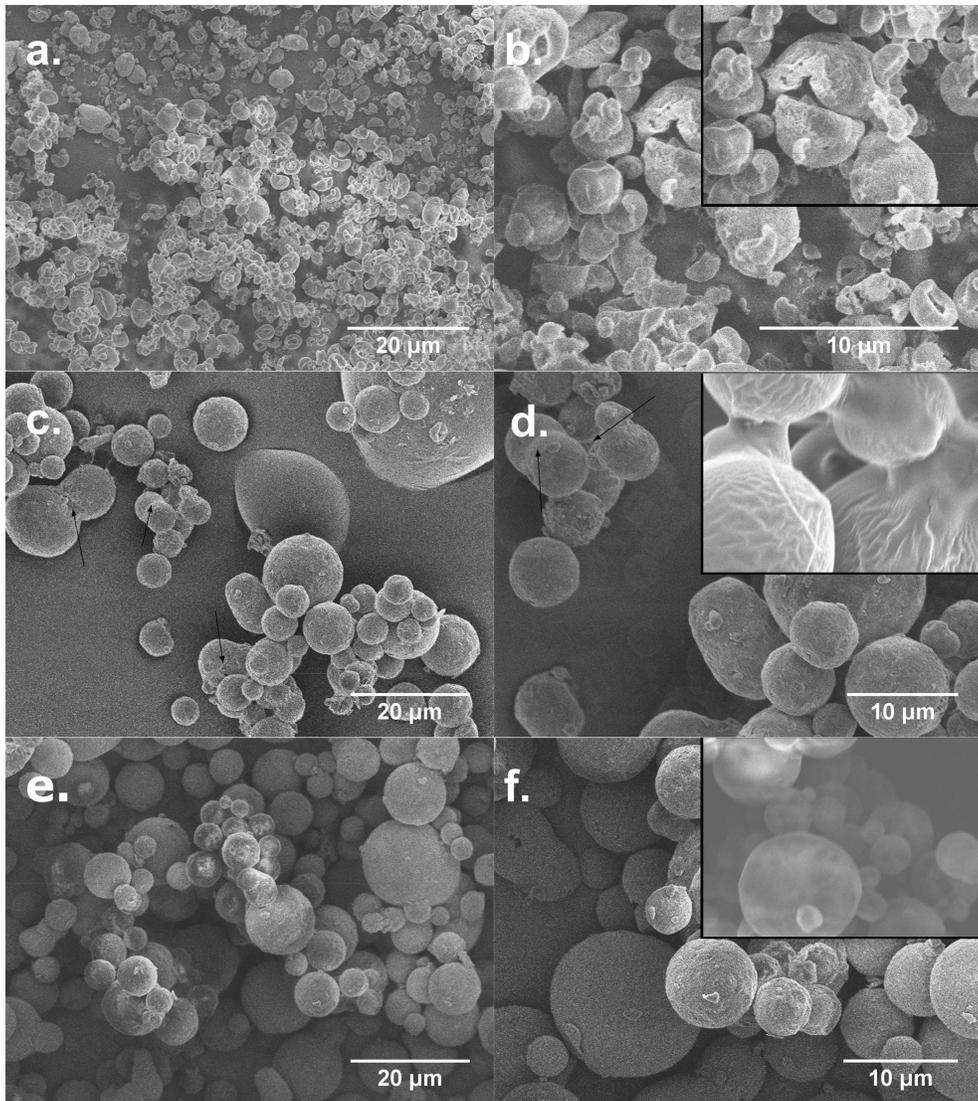
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Figure 1. Schematic diagram of the spray drying process. Labeled components are 1) the spray dryer nozzle, 2) the spray drying chamber, 3) the separating cyclone and 4) the collection chamber.



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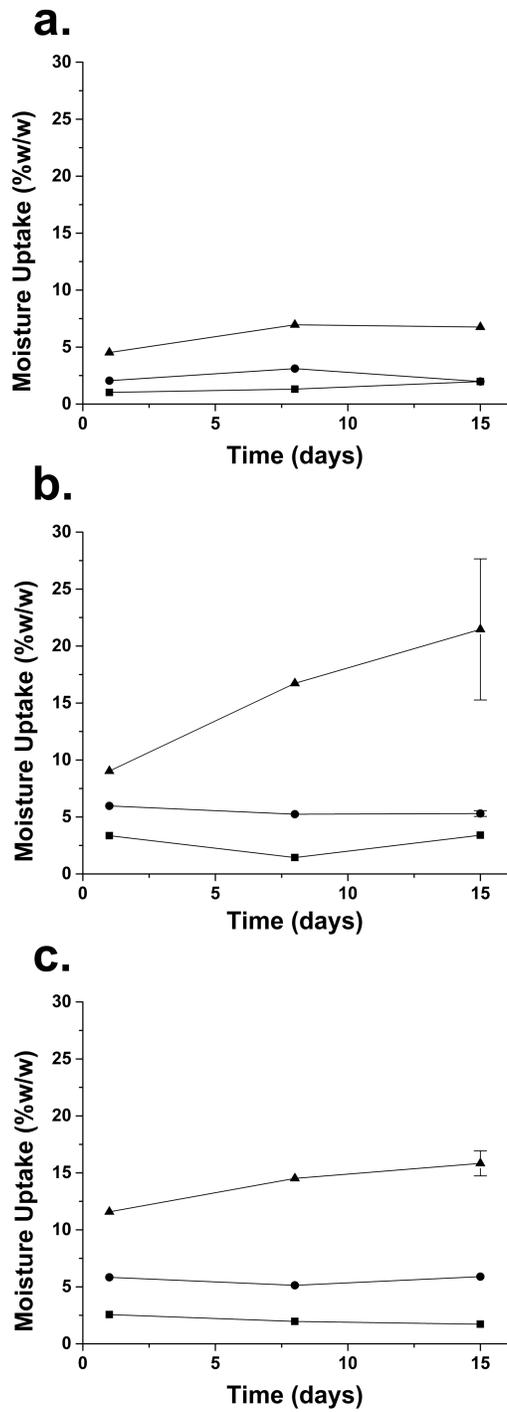
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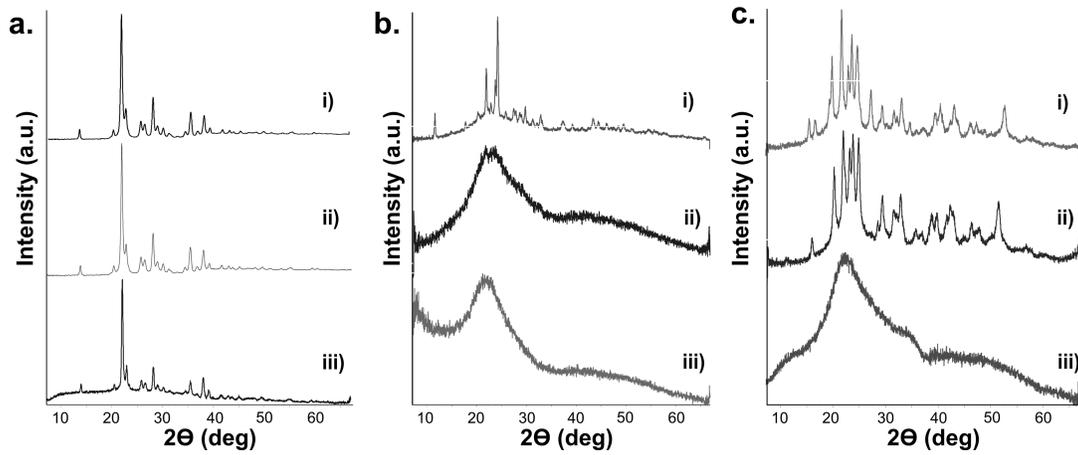
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Figure 2: Spray dried particles imaged by scanning electron microscopy composed of L-leucine (a,b), lactose/trehalose (c,d) and mannitol/dextran (e,f). Insets shown detail particle bridging when present at electron microscope magnifications of 5000x (panel b) and 10000x (panels d, f). These spray dried formulations do not contain adenoviral vector.



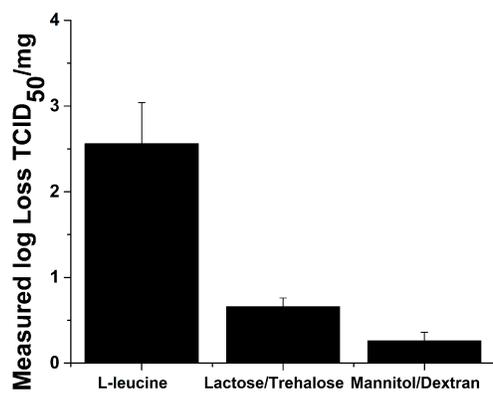
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Figure 3: Moisture uptake (wt. %) of L-leucine (a), lactose/trehalose (b) and mannitol/dextran (c) formulations after storage for up to two weeks at 20°C and relative humidities of <10% (□), 45% (◻) and >90% (◄). Data is shown as mean (± SD).



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Figure 4: X-ray diffraction peak crystal intensities (arbitrary units) measured across a range of x-ray incidence angles for L-leucine (a), lactose/trehalose (b) and mannitol/dextran (c) formulations. Storage conditions are immediately post spray drying (i), two weeks storage at 20°C and <10% RH (ii) and two weeks storage at 20°C and 45% RH (iii).



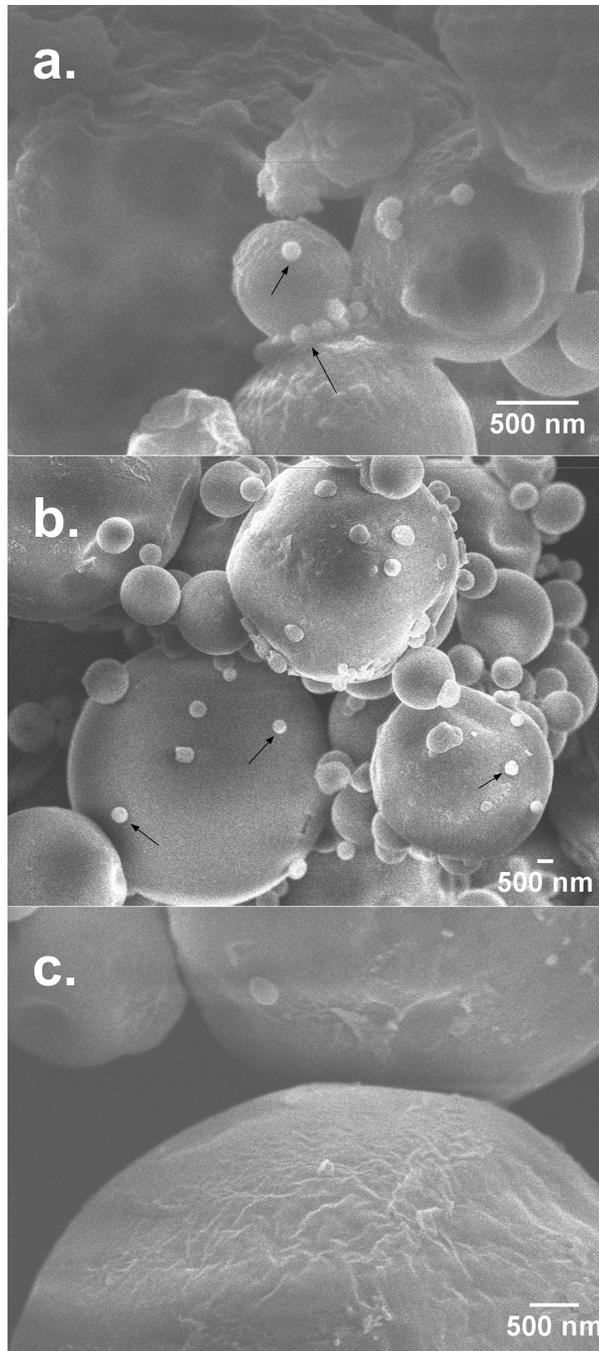
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Figure 5: Measured loss of AdHu5 infectivity for L-leucine, lactose/trehalose and mannitol/dextran, formulations after spray drying (i.e. process loss at t=0 days). Data is shown as mean ± SD (n = 3).

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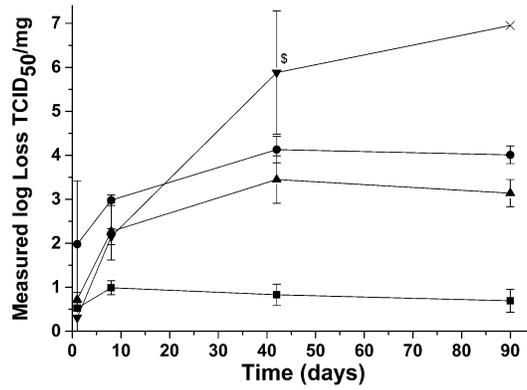
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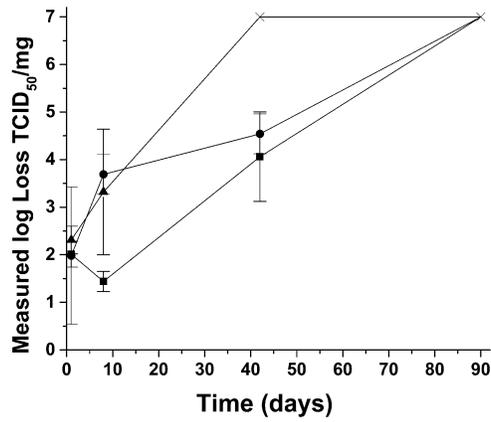
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Figure 6: SEM micrographs of formulations spray dried with adenoviral vector: L-leucine (a), lactose/trehalose (b) and mannitol/dextran (c). Proposed AdHu5 nodules present on the particle surface are indicated by black arrows.



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Figure 7: Measured log loss of AdHu5 vector infectivity after storage up to 90 days at 20°C and <10% RH for liquid control (□), L-leucine (□), lactose/trehalose (□) and mannitol/dextran (□), formulations. Initial time point is at t=1 day. Three repeat samples were stored for each formulation and ^{\$} denotes viral activity below the detection limit for one repeat and 'x' denotes viral activity below the detection limit for all repeats. Data is represented as mean ± SD for three repeat samples and mean ± range for two repeat samples.



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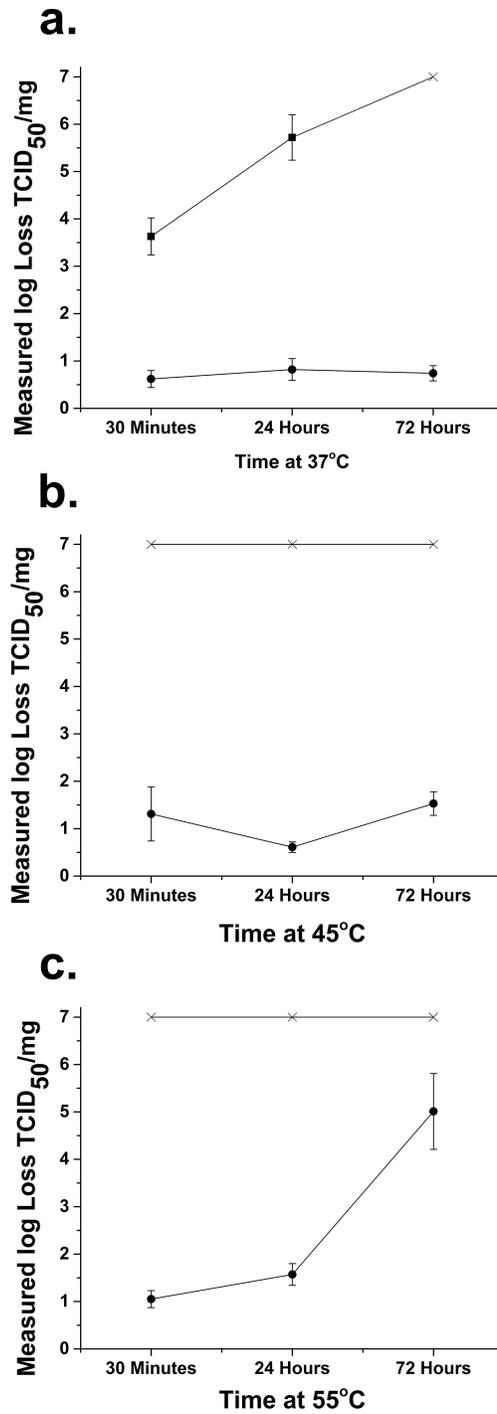
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Figure 8: Measured log loss of AdHu5 vector infectivity after storage up to 90 days at 20°C and 45% RH for L-leucine (□), lactose/trehalose (□) and mannitol/dextran (□) formulations. Initial time point is at t=1 day. Three repeat samples were stored for each formulation and 'x' denotes viral activity below the detection limit for all repeats. Data is represented as mean ± SD for three repeat samples.



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Figure 9: Measured AdHu5 infectivity loss for both control (□) and mannitol/dextran formulation (□) at a storage of 37°C (a), 45°C (b) and 55°C (c) for up to three days. Three repeat samples were stored for each formulation and 'x' denotes viral activity below the detection limit for all repeats. Data is represented as mean +/- SD for three repeat samples and mean +/- range for two repeat samples.